

## An investigation on peristaltic flow of nanofluids: Application in drug conveyance frameworks

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**ABSTRACT:** This paper studies the peristaltic flow of nanofluids through a two-dimensional channel. The analysis is conducted based on the long wavelength and low Reynolds number approximations. The walls of the channel surface propagate sinusoidally along the channel. The Buongiorno formulation for nanofluids is employed. Approximate analytical solutions for nanoparticle fraction field, temperature field, axial velocity, volume flow rate, pressure gradient and stream function are obtained. The impact of the pertinent physical parameters i.e. thermal Grashof number, basic-density Grashof number, Brownian motion parameter and thermophoresis parameter on nanoparticle fraction profile, temperature profile, velocity profile and trapping phenomenon are computed numerically. The results of this study demonstrate good correlation with the Newtonian results of Shapiro et al. (1969) [4], which is a special case ( $GrT = 0$ ,  $GrF = 0$ ) of the generalized model developed in this article. Applications of the study include peristaltic micro-pumps and novel drug delivery systems in pharmacological engineering.

**KEYWORDS:** Peristaltic flow, Nanofluids, Grashof numbers, Brownian motion, Thermophoresis, Peristaltic pumps, Pharmacology.

### I. INTRODUCTION

Peristaltic pumping is a form of fluid transport which is achieved via a progressive wave of contraction or expansion which propagates along the length of a distensible tube containing fluids. In general, this pumping takes place from a region of lower pressure to higher pressure. It is an inherent property of many of the smooth muscle tubes such as the gastrointestinal tract, male reproductive tract, fallopian tube, bile duct, ureter and oesophagus. The principle of peristaltic transport is also exploited in many industrial applications. These include sanitary fluid transport, transport of corrosive fluids, blood pumps in heart lung machines, novel pharmacological delivery systems etc. Since the experimental work of Latham [1], many investigations [2–4] dealing with peristaltic flow for different flow geometries and under various assumptions, have been presented by employing analytical, numerical and experimental approaches. Fung and Yih [2], who presented a model on peristaltic pumping using a perturbation technique, associated reflux with net backward flow. Barton and Raynor [3] studied the peristaltic motion in a circular tube by using the long wavelength approximation for intestinal flow. Shapiro et al. [4] extended their work for the steady flow of Newtonian fluids through the channel and tube with sinusoidal wall propagation and theoretically evaluated the reflux and trapping phenomena. The fluids present in the ducts of a living body can be classified as Newtonian and non-Newtonian fluids based on their shear-stress-strain behavior. Peristaltic transport on a microfluid scale has also received attention. Important studies of micro-peristaltic pumps include Quake and Scherer [5] who have reported pneumatic valves constructed in multilayer polydimethylsiloxane (PDMS) devices. These PDMS valves comprise overlapped fluidic and control channels (that reside in different layers) which are separated by a thin polymeric membrane. Increased pressure in the control channel results in the deformation of the PDMS membrane and closing of the fluidic channel. Simple valves and peristaltic pumps produced by a series of valves have been demonstrated using this technology. Chou et al. [6] have described micro-peristaltic pumps which comprise two PDMS layers that are permanently bonded together. Fluidic channels that are 100  $\mu\text{m}$  wide and 10  $\mu\text{m}$  height (measured in the center of the channel) are formed within a thin film (30  $\mu\text{m}$ ) of PDMS. Control lines (200  $\mu\text{m}$  wide) are molded in a thick layer (5000  $\mu\text{m}$ ) of PDMS and positioned above the fluidic channels. A thin membrane of polymer delineates the fluidic and control channels and permits the actuation of peristaltic pumps and valves. Mathematical simulations of such devices are therefore of great industrial importance. In numerous peristaltic pumps, heat

transfer also plays an important role and is strongly influenced by peristaltic flow fields. The influence of heat transfer on peristaltic flow of Newtonian and non-Newtonian fluids has been reported for various geometrical configurations by for example, Vajravelu et al. [7] who considered a vertical porous annulus. Kothandapani and Srinivas [8] examined hydromagnetic heat transfer in peristaltic flow in a porous medium. Mekheimer and Abdelmaboud [9] simulated the magneto-convective peristaltic flow in a vertical annulus. Hayat et al. [10] studied peristaltic magneto-convection in a porous medium channel. Akbar and Nadeem [11] derived solutions for viscoelastic chemically-reacting peristaltic flow and heat transfer in a stenotic vessel. Further studies include the recent investigations by Tripathi [12,13] and Tripathi et al. [14,15] for the dynamics of swallowing with thermal transport effects. Transient peristaltic flows have also been considered by Pandey and Tripathi [16–18] for a diverse spectrum of non-Newtonian fluids. Peristaltic flow of viscoelastic fluids with different fractional models have additionally also received some attention, as elaborated in [19–23]. In recent years a new branch of fluid mechanics has emerged, namely nanofluid dynamics, which finds diverse applications in medical science, energetics, biology and process systems engineering. Initial developments were made by Choi [24] in the realm of energy performance enhancement. Nanofluids as elucidated by Xuan and Li [25] are a new class of fluids that are engineered by suspending nanoparticles (NP) in “base” heat transfer fluids. Nanofluids are synthesized by dispersing the nano particles (NP) (nanometer-sized particles i.e.  $<100$  nm) in the base fluid such as water ( $H_2O$ ), ethylene-glycol (EG), or propylene-glycol (PG), coolants, biofluids, emulsions, oil, lubricants and silk fibroin (SF). A creative combination of nanoparticles and liquid molecules are shown in Fig. 1. Although the concept of nanofluids was first proposed by the great Scottish theoretical physicist, James Clerk Maxwell in the late 19th century, more than a century later the term “nanofluid” was officially introduced by the energy scientist Choi [24] who fabricated such nanofluids at the Argonne National Laboratory, Energy Technology Division based in Illinois, USA. Choi, in 1995 [24] pioneered the development of such fluids containing suspensions of nanometer-sized particles and disclosed their significant thermal properties through the measurement of the convective heat transfer coefficient of those fluids. Various benefits of the application of nanofluids, such as improved heat transfer, size reduction of the heat transfer system, minimal clogging, microchannel cooling, and miniaturization of systems, were achieved in his study. Since then investigations have been continued and recent potential identified in the biomedical device and pharmaceutical industries. Both convection and conduction heat transfer modes have been addressed in detail. Xuan and Li [25] measured convective heat transfer coefficients for Cu/water nano-fluids, and found substantial heat transfer enhancement. Lee et al. [26], measured conductive heat transfer coefficients of  $Al_2O_3$ /water,  $Al_2O_3$ /ethylene-glycol, CuO/water, and CuO/ethylene-glycol nanofluids. Pak and Cho [27] investigated convective heat transfer in the turbulent flow regime using  $Al_2O_3$ /water and  $TiO_2$ /water nanofluids, and observed that the Nusselt number of the nanofluids increased with increasing volume fraction of the suspended nanoparticles, and also with increasing Reynolds number. Lee and Choi [28] studied convective heat transfer of laminar flow of an unspecified nanofluid in microchannels. Nanofluids were also observed to have the ability to dissipate heat power three times more effectively than pure water. Bég et al. [29] simulated numerically the unsteady magnetized nanofluid polymeric synthesis from a stretching sheet using Maple software, identifying the strong influence of time on nano-particle distributions. Zienali et al. investigated the convective heat transfer of  $Al_2O_3$ /water and CuO/water-based nanofluids in circular tubes, and observed that the heat transfer coefficient was enhanced by increasing the concentration of nanoparticles in the nanofluids. Bég et al. [31] utilized a homotopy semi-computational algorithm to evaluate the thermal and nano-particle concentration boundary layer growth in the low-order stagnation-point regime of a sphere embedded in porous media. Maiga et al. [32] studied numerically the heat transfer enhancement in turbulent tube flow using  $Al_2O_3$  nanoparticles suspension. Buongiorno [33] presented a seminal analysis of convective transport in nanofluids using non-dimensionalization; this study has laid the foundations for numerous subsequent analytical and numerical investigations including Kuznetsov and Nield [34,35], Kolade et al. [36], Kakaç and Pramuanjaroenkij [37] and Bachok et al. [38]. More complex nanofluid transport processes have been considered by Uddin et al. [39] who employed Lie group algebra and numerical methods to compute the influence of nanofluid rheology on thermofluid and mass transfer characteristics in heat-generating boundary layer flows. Bég et al. [40] simulated via a Chebyshev spectral collocation scheme, the electrohydrodynamic propulsion of nanofluids in drug delivery, evaluating the effects of electrical Hartmann number and electrical Reynolds number. A detailed review of progress in numerical simulation of nanofluid dynamic flows in biomechanics (renal and transdermal transport) has been presented very recently by Bég et al. [41], who have also employed single and two-phase particulate models and finite volume algorithms to evaluate the three-dimensional transport behavior in bio-nano-polymer drug flows. Very few studies of peristaltic transport of nanofluids are available however in the literature, despite important applications in medical engineering systems. We quote here the very recent study by Akbar et al. [42] who studied peristaltic flow of a nanofluid in a diverging tube, coupling the temperature and nanoparticle equations using a homotopy perturbation method. They showed that pressure rise decreases with the increase in thermophoresis number whereas elevating the Brownian motion

parameter and the thermophoresis parameter induces a rise in temperatures the purpose of the present paper is to describe the influence of nanoparticles on heat transfer and peristaltic flow through a two-dimensional channel. The problem is simplified by taking the low Reynolds number and long wavelength approximation. Solutions are benchmarked with the previous Newtonian, non-thermal study of Shapiro et al. [4]. The effects of thermal Grashof number, basic-density Grashof number, Brownian motion parameter and thermophoresis parameter on nanoparticle fraction profile, temperature profile, velocity profile, and stream line distribution are discussed with the aid of computational illustrations. This model is applicable to the simulation of particle flows in hemodynamic transport in small vessels and also nanofluid peristaltic pumps in biochemical and medical engineering. It is envisaged that the present study.

## II. MATHEMATICAL MODEL

The constitutive equation for the wall geometry (cf. Fig. 2) where  $q_f$ ;  $q_p$ ;  $l$ ,  $g$ ,  $b$ ,  $(q_c)_f$ ,  $(q_c)_p$ ,  $k$ ,  $T$ ,  $F$ ,  $DB$ ,  $DT$  and  $q_0$  denote the fluid density, nanoparticle mass density, axial velocity, transverse velocity, transverse coordinate, pressure, fluid viscosity, acceleration due to gravity, volumetric expansion coefficient of the fluid, heat capacity of fluid, effective heat capacity of nanoparticle, thermal conductivity, temperature, nanoparticle volume fraction, Brownian diffusion coefficient, thermophoretic diffusion coefficient, and the nanofluid density at the reference temperature ( $T_0$ ). We then introduce the following non-dimensional parameters

## III. NUMERICAL RESULTS AND DISCUSSION

The geometry of the peristaltic nanofluid regime is illustrated in Fig. 2. In this section, the influence of pertinent nanofluid characteristics on the peristaltic flow pattern is studied graphically. All illustrations have been generated with the Mathematica software. The effects of Brownian motion parameter ( $N_b$ ) and thermophoresis parameter ( $N_t$ ) on nanoparticle fraction profile ( $U(g)$ ) and temperature profile ( $h(g)$ ) are presented through Figs. 3 and 4. The Brownian motion parameter,  $N_b$ , arises in the energy and species (nano-particle volume fraction) conservation equations i.e. Eqs. (11) and (12), via the mixed derivative term, former, and the second order temperature derivative, in the latter. Clearly  $N_b$  is an important parameter therefore influencing the species diffusion. Fig. 3(a) shows that with an increase in Brownian motion parameter ( $N_b$ ), there is a strong decrease in nanoparticle fraction profile  $U(g)$ . The nanofluid behaves more like a fluid than the conventional solid-fluid mixtures in which relatively larger particles with micrometer or millimeter orders are suspended. The nanofluid is a two-phase fluid in nature and random movement of the suspended nanoparticles increases energy exchange rates in the fluid but depresses concentrations in the flow regime. We also note that with greater values of dimensionless transverse coordinate,  $g$ , there is a pronounced divergence in profiles i.e. as we migrate from the channel centerline ( $g = 0$ ), the profiles move apart. This trend has also been observed by Akbar et al. [42]. Thermophoretic parameter ( $N_t$ ) effects are depicted in Fig. 3(b). A marked elevation in  $U(g)$  values accompanies an increase in  $N_t$  from 1 to 4. As with the Brownian motion parameter,  $N_t$  also arises in both energy and nanoparticle volume concentration conservation equations (11) and (12), respectively. Although it features in the same term in the latter as  $N_b$ , in the former (Eq. (11)) it appears in a separate term, consistent with the original formulation of Buongiorno [33], viz. Hence species diffusion is accentuated with thermophoresis. This pattern is also consistent with macroscopic convection flows (non-nanofluid), as indicated by Zueco et al. [43]. Similar results have also been obtained in nanofluid studies by, for example Kuznetsov and Nield [34] among others, and more recently by Uddin et al. [39] using a novel differential transform semi-numerical code. The positive influence of  $N_t$  on  $U(g)$  profiles is only apparent however for  $g > 1$ . Prior to this the effect is reversed and close to the longitudinal axis of the channel the nano-particle concentrations are in fact depressed with thermophoresis. This unusual response has also been identified by Akbar and Nadeem [44], although actual elucidation requires experimental investigations. It indicates that both  $N_b$  and  $N_t$  have a similar effect on temperature distributions in the flow regime for some transverse distance from the channel centre, temperature  $h(g)$  is initially enhanced with Brownian motion and with thermophoresis i.e. the regime is heated. However for  $g > 1$ , the trends are reversed. As we approach the periphery of the channel, Brownian motion and thermophoresis tend to depress temperatures i.e. they act to cool the regime. Thermophoresis is the migration of nanoparticles in the direction of a decreasing temperature gradient. Evidently this phenomenon has a potent effect on temperature evolution throughout the channel cross-section. Fig. 5(a)–(e) show that axial velocity ( $u$ ) is generally negative for the channel half-space defined by  $0 \leq g \leq 1$ ; flow reversal i.e. back-flow is therefore taking place. Maximum velocities are always located at the channel centre, decaying smoothly to zero at the periphery (channel wall).

Fig. 5(a) indicates that an increase in Brownian motion parameter,  $N_b$ , decreases magnitudes of the axial velocity i.e. opposes backflow  $u$ -values therefore become more positive. The flow is therefore decelerated with Brownian motion. A similar response is computed for the effect of thermophoresis parameter in Fig. 5(b). Fig. 5(c) shows the effect of thermal Grashof number ( $Gr_T$ ) on axial velocity distribution. This parameter signifies the relative influence of thermal buoyancy force and viscous hydrodynamic force. For  $Gr_T <$

1, the peristaltic regime is dominated by viscous forces and vice versa for  $Gr_T > 1$ . For the intermediate case of  $Gr_T = 1$  both thermal buoyancy and viscous forces are of the same order of magnitude, as described by Béget al. [45]. Velocity magnitudes are generally reduced with increasing thermal Grashof number. The profiles follow monotonic patterns for  $0.5 < Gr_T < 1.5$ . However with  $Gr_T = 2$ , an undulating profile is observed from the channel centerline to the wall. Thermal buoyancy generally serves to retard the flow in the regime. Fig. 5(d) reveals that the influence of the species (basic-density) Grashof number,  $Gr_F$ , is opposite to that of the thermal Grashof number. Increasing  $Gr_F$ , acts to increase magnitudes of the axial velocity i.e. exacerbates the backflow in the regime.  $Gr_F$  represents the ratio of species buoyancy force to the viscous hydrodynamic

#### IV. CONCLUSIONS

The influence of nanofluid characteristics on peristaltic heat transfer in a two-dimensional axisymmetric channel have been studied analytically with the aid of Mathematica software. The study has been motivated by applications in novel nanofluid drug delivery systems in the digestive system. Numerical computations have shown that: Increasing Brownian motion parameter ( $N_b$ ), reduces nano-particle fraction profile  $U(g)$ , whereas thermophoretic parameter enhances ( $N_t$ ) it. Temperature  $h(g)$  is initially enhanced with Brownian motion and with thermophoresis i.e. the regime is heated. Increasing Brownian motion parameter,  $N_b$ , and thermophoretic parameter ( $N_t$ ) suppress axial velocity ( $u$ ) i.e. oppose backflow. Axial velocity ( $u$ ) magnitudes are generally reduced with increasing thermal Grashof number whereas the converse behaviour is caused with increasing species Grashof number ( $Gr_F$ ). Nanofluids tend to suppress backflow compared with Newtonian fluids. Increasing Brownian motion parameter ( $N_b$ ) reduces pressure difference, whereas increasing thermophoretic parameter ( $N_t$ ) strongly enhances pressure difference, for all values of averaged volume flow rate,  $Q$ . Increasing thermal and species (basic-density) Grashof numbers elevates pressure difference for all flow rates. The magnitude of trapped bolus is decreased with increasing the magnitude of Grashof numbers. Decreasing Brownian motion parameter reduces the number of boluses trapped. Decreasing thermophoretic parameter, causes the size of boluses to be slightly increased i.e. reduces the reflux region. With decreasing thermal Grashof number bolus size is increased. An increase in species Grashof number has a similar effect to reducing Brownian motion parameter i.e. the dual bolus structure is reduced to a single bolus. The current study has examined a horizontal channel, neglecting gravitational effects. Future investigations will consider nano-fluid three-dimensional (3-D) peristaltic flows in an inclined channel and will be communicated imminently. Furthermore it is hoped that the present investigation will further stimulate researchers interesting in conducting experiments on nanofluid peristaltic transport phenomena, which would provide a much-needed framework for validating mathematical models.

#### REFERENCES

- [1]. T.W. Latham, Fluid motion in a peristaltic pump, MS Thesis, MIT, USA, 1966.
- [2]. Y.C. Fung, C.S. Yih, Peristaltic transport, ASME J. Appl. Mech. 35 (1968) 669–675.
- [3]. C. Barton, S. Raynor, Peristaltic flow in tubes, Bull. Math. Biophys. 30 (1968) 663–680.
- [4]. A.H. Shapiro, M.Y. Jafferin, S.L. Weinberg, Peristaltic pumping with long wavelengths at low Reynolds number, J. Fluid Mech. 37 (1969) 799–825.
- [5]. S.R. Quake, A. Scherer, From micro- to nano-fabrication with soft materials, Science 290 (2000) 1536–1540.
- [6]. H.P. Chou, M.A. Unger, S.R. Quake, A microfabricated rotary pump, Biomed. Microdevices 3 (2001) 323–330.
- [7]. K. Vajravelu, G. Radhakrishnamacharya, V. Radhakrishnamurthy, Peristaltic transport and heat transfer in a vertical porous annulus with long wave approximation, Int. J. Non-Linear Mech. 42 (2007) 754–759.
- [8]. M. Kothandapani, S. Srinivas, On the influence of wall properties in the MHD peristaltic transport with heat transfer and porous medium, Phys. Lett. A 372 (2008) 4586–4591.
- [9]. Kh.S. Mekheimer, Y. Abdelmaboud, The influence of heat transfer and magnetic field on peristaltic transport of a Newtonian fluid in a vertical annulus: application of endoscope, Phys. Lett. A 372 (2008) 1657–1665.
- [10]. T. Hayat, M.U. Qureshi, Q. Hussain, Effect of heat transfer on the peristaltic flow of an electrically conducting fluid in porous space, Appl. Math. Model. 33 (2008) 1862–1873.
- [11]. N.S. Akbar, S. Nadeem, Simulation of heat and chemical reactions on Reiner-Rivlin fluid model for blood flow through a tapered artery with a stenosis, Heat Mass Transfer 46 (2010) 531–539.
- [12]. D. Tripathi, A mathematical model for swallowing of food bolus through the oesophagus under the influence of heat transfer, Int. J. Therm. Sci. 51 (2012) 91–101.
- [13]. D. Tripathi, Study of transient peristaltic heat flow through a finite porous channel, Math. Comput. Model. 57 (2013) 1270–1283.
- [14]. D. Tripathi, S.K. Pandey, O. Anwar Béget, Mathematical modelling of heat transfer effects on swallowing dynamics of viscoelastic food bolus through the human oesophagus, Int. J. Therm. Sci. 70 (2013) 41–53.
- [15]. D. Tripathi, O. Anwar Béget, A study of unsteady physiological magneto-fluid flow and heat transfer through a finite length channel by peristaltic pumping, Proc. Inst. Mech. Eng., Part H, J. Eng. Med. 226 (8) (2012) 631–644.
- [16]. S.K. Pandey, D. Tripathi, A mathematical model for peristaltic transport of micro-polar fluids, Appl. Bionics Biomech. 8 (2011) 279–293.
- [17]. S.K. Pandey, D. Tripathi, Peristaltic transport of a Casson fluid in a finite channel: application to flows of concentrated fluids in oesophagus, Int. J. Biomath. 3 (2010) 473–491.
- [18]. S.K. Pandey, D. Tripathi, Influence of magnetic field on the peristaltic flow of a viscous fluid through a finite-length cylindrical tube, Appl. Bionics Biomech. 7 (2010) 169–176.
- [19]. D. Tripathi, A mathematical model for the peristaltic flow of chyme movement in small intestine, Math. Biosci. 233 (2011) 90–97.
- [20]. D. Tripathi, Numerical study on creeping flow of Burgers' fluids through a peristaltic tube, ASME J. Fluids Eng. 133 (2011)

- 121104-1–121104-9.
- [21]. D. Tripathi, Numerical study on peristaltic flow of generalized Burgers' fluids in uniform tubes in presence of an endoscope, *Int. J. Numer. Methods Biomed. Eng.* 27 (2011) 1812–1828.
- [22]. D. Tripathi, Peristaltic transport of fractional Maxwell fluids in uniform tubes: application of an endoscope, *Comput. Math. Appl.* 62 (2011) 1116–1126.
- [23]. D. Tripathi, Numerical study on peristaltic transport of fractional bio-fluids, *J. Mech. Med. Biol.* 11 (2011) 1045–1058.
- [24]. S.U.S. Choi, Enhancing thermal conductivity of fluid with nanoparticles, in: D.A. Siginer, H.P. Wang (Eds.), *Developments and Application of Non-Newtonian Flows*, 66, ASME, New York, 1995, pp. 99–105.